

Clinical significance and various role of Perfusion Index in the disease management – A review

Sanjeev Kumar

Research Scholar, IEC University, Baddi, Solan, Himachal Pradesh

Date of Submission: 20-07-2024

Date of Acceptance: 30-07-2024

ABSTRACT

In the fields of anaesthesia, perioperative care, and critical care, photoplethysmography (PPG) has been widely utilised for pulse oximetry monitoring. Certain PPG signal components, however, have been used for different objectives, such as noninvasive hemodynamic monitoring. The ratio of pulsatile to nonpulsatile light absorbance or reflectance of the PPG signal is represented by the perfusion index (PI), which is obtained from the PPG signal. The intricate and interconnected peripheral determinants of and central hemodynamic features, including vascular tone and stroke volume, are reflected in the PI determinants. Numerous research conducted recently have shown the intriguing functions of this variable, particularly in the evaluation of regional or neuraxial block success and hemodynamic monitoring in anaesthesia, perioperative care, and critical care. However, as of yet, no evaluation has been released regarding PI's interest in these subjects. The physiological and pathologic factors that determine PI will be discussed first in this narrative overview, followed by the mean used to calculate this number and any possible restrictions. The evidence that is currently available about the effectiveness of PI in various clinical settings, including operating rooms, critical care units, and emergency departments, will be given and addressed in the second section. Lastly, the viewpoints on the use of PI and the points that need to be investigated in relation to this instrument will be highlighted.

I. INTRODUCTION

Takuo Aoyagi, who died on April 18, 2020, created pulse oximetry in the 1970s by utilising red and infrared light transmission through tissues in accordance with earlier research [1]. The fields of anaesthesia, perioperative care, and critical care have seen an increase in interest in non-invasive macrohaemodynamic and microcirculation monitoring. The photoplethysmography (PPG) signal, which was previously limited to monitoring oxygen saturation for decades, is now a useful tool for monitoring hemodynamics. PPG is an

----inexpensive, quick, easy-to-use, non-invasive tool. PPG data interpretation, however, can be difficult. The early use of this multifunctional device for hemodynamic monitoring via PPG signal was flawed due to a significant ignorance of its drivers. Nonetheless, PPG signal analysis has benefited from renewed interest in recent years, and several studies in anaesthesia, perioperative care, and critical care have demonstrated the value of PPG [2-4]. Perfusion index (PI), which is the percentage of the pulsatile element of PPG among other PPG signal components, has been extensively examined and is a potentially useful tool for medical professionals. Therefore, to maximise its proper use and effectiveness, one must have a solid grasp of the PI and PPG determinants as well as its constraints. This review will go on to describe physiological factors of PI as well as physical concepts. A number of PPG evaluations have been put up, most notably regarding the respiratory fluctuations of PI, also known as Pleth Variability Index (PVI), and its uses [3, 5–7]. But none of the evaluations listed above concentrated on PI specifically. Since then, a number of fresh data sets have also been released. This study provides the clinical use of PI in the operating room, perioperative care, and critical care. It also includes the physiological and technological components of PPG and PI that physicians need to grasp.

Measurement of Perfusion Index

• Principles and mechanisms of photoplethysmography

Conventional PPG works on the basis of measuring changes in tissue volume indirectly through changes in the absorption of light beams passing through the tissue. After entering a tissue, the oximeter probe produces red and ultra-red light beams whose transmitted intensities are converted into an electrical current by a photodetector [8,9]. The same approach applies to another PPG modality called PPG via reflection, which makes advantage of the tissue's light reflecting capabilities. After that, the photodetector is positioned close to the light source to gauge the



incident beams' reflectance [10]. PPG often uses two wavelengths: infrared light (940 nm) and red light (660 nm), which are mostly absorbed by oxyhaemoglobin and deoxyhaemoglobin, respectively. Variations in infrared light absorption are used to obtain the PPG curve. Nonetheless, some PPG devices employ one wavelength, or sometimes more than two [11].

• Components of Perfusion Index

Absorption of light fluctuates during the cardiac cycle. The maximum absorption occurs during the systole, which is indicative of the dilatation of arteries caused by the systolic pressure-that is, the rise in arterial blood volume under the illumination. The photodetector first receives the signal, which is then divided into pulsatile and non-pulsatile signals. During systole, pulsatile fluctuations in light absorption are sometimes described to as "alternating current" (AC). AC is the total of the fluctuations in the diameters of the pulsatile vessels that the light beams travel through. It indicates variations in the absorbance or reflectance of the incident light beams caused by pulsatile vessels under variations in arterial pressure. After signal processing, the PPG curve shown on real displays depicts AC, which is obtained from the infrared light stream. In order to decrease signal artefacts and achieve restoration of AC, computer filters must process the raw signal that the photodetector received [8,12,13]. Conversely, constant absorption is known as "direct current" (DC), and it is from DC that AC fluctuates. DC is the same as light absorption from other tissues such skin, soft tissues, bones, and non-pulsatile capillaries and venous arteries. Currently, DC is not shown on standard oximeter monitors. The PPG curve can be considerably distorted by these manufacturerdependent methods between manufacturers [8,9].

• Calculation of Perfusion Index

PI stands for the ratio, or AC/DC, of continuous light absorption to pulsatile light absorption. PI, sometimes known as "peripheral PI," was first employed in pulse oximetry as a high-quality signal indication [4,14]. On the other hand, PI reflects the fluctuation in local blood volume during systole and is dependent on both the local and systemic hemodynamic state. Therefore, non-invasive hemodynamic monitoring may be achieved using PI.

• Perfusion Index's Physiological value

Two investigations reported mean PI levels (\pm standard deviation) at the finger (in healthy awake participants) of 2.2% \pm 2.0 and 3.5% \pm 2.4 [15, 16]. According to this, AC only makes up 2% to 3% of DC. In terms of vascular physiology, this indicates that the blood volume underneath the sensor rises by 2% with each pulse.

However, it is challenging to suggest a trustworthy normal value for this parameter because of the large differences in normal values among healthy volunteers (from < 1% to > 10%).

• Significance of Direct Current (DC)

Any change in DC will cause a fluctuation in PI since PI is the ratio of AC to DC. Therefore, venous compression (by, for example, a finger clip) or soft tissues may reduce DC and raise PI. Similarly, congestion brought on by an excess of fluid in the world would have the opposite effect. PI value would also be impacted by limb position owing to variations in venous filling and, therefore, DC; if the limb is in a declive position (venous congestion), DC would rise, and if it is in a proclive position, DC will decrease [3]. From a physiological standpoint, DC is also not continuous; in patients breathing on their own or with mechanical ventilation, minor fluctuations in sympathetic tone and venous return are noted [17, 18]. Likewise, DC may alter in response to alterations in vascular tone, such as those caused by vasoactive medications (i.e., DC reduction in response to elevated vascular tone) [19].

• Alternating current (AC)

According to some writers, PI just serves as a stand-in for vascular tone. A reliable proxy for vascular tone, the central to toe temperature gradient, was found to be linked with PI by Lima et al. [15]. In fact, PI quickly rose in the occluded region following local vasodilation brought on by plexus or spinal anaesthesia. In patients undergoing general anaesthesia, alterations in vascular tone caused by vasopressors (i.e., a drop in PI as a result of norepinephrine infusion) also had a significant impact on PI [20-25]. In fact, a number of recent investigations have indicated that stroke volume, or SV, is yet another significant PI predictor. In babies, PI was connected with both cardiac output and superior vena cava flow [26-28]. Although such information is not included in these papers, reduced flow may be linked to elevated vascular tone. Healthy individuals were subjected to a lower body negative pressure by Van Genderen et al.



[29]. As reported as median and interquartile, they saw a sharp decline in PI (from 2.2% [1.6–3.3] to 1.3% [0.9–1.7]), a drop in SV, and no discernible rise in the skin temperature differential between the forearm and fingertip. The absence of substantial changes in the skin temperature gradient between the fingertip and forearm may be attributed to temperature change inertia or the small research sample (25 male participants). This suggested that SV itself had an impact on PI in addition to the local vascular tone [29-35].

Local conditions

Local perfusion is evaluated by PI measurement. Even for clothe locations, the PI value varies by a few centimetres depending on the measurement site [33]. Thus, both local and systemic macrohaemodynamic state have a significant impact PI. Given on that thermoregulation and non-thermoregulatory stimuli (such as nociception and exercise) mostly affect local vascular tone [36,37]. For instance, following cold exposure, PPG waveform variance varied significantly between the ear and the finger [38]. Another way that regional anaesthesia demonstrates the impact of local conditions is through the increase in PI measured in the blocked area following the procedure. This indicates a decrease in local vascular tone, which is linked to an increase in local blood flow and volume in the blocked area with each heartbeat. The rise in AC and PI values is being caused by both the decrease in vascular tone and the increase in local blood flow and volume. Although this hasn't been researched, it is anticipated that DC will rise in the blocked area along with other vascular tone alterations. PI is a tool for monitoring local hemodynamics in this scenario, not central hemodynamics. Similarly, a variety of local factors need to be taken into account when interpreting a PI measurement, including local compression of soft tissues, veins, and/or arteries, changes in external temperature, limb postures, and severe arterial abnormalities such obliterating arteriopathy. Peripheral PI in the aforementioned circumstances more closely represents local circumstances than the central hemodynamic state [11, 27]. But there was no change in basal PI between individuals with and without vascular illness (diabetes and hypertension). Conversely, depending on the test site, macrohaemodynamic state, or cardiac index, might affect PI value. In fact, for low cardiac output in babies, PI tends to be larger at the right hand than the foot, and inversely

for high cardiac output [26]. All of these factors point to the significance of regional variations in perfusion on local PI values, which are due to changes in sympathetic response and central hemodynamic condition [39].

Clinical uses

In a variety of therapeutic contexts, PI has been investigated in the operating room for patients receiving general or regional anaesthesia.

• PI in evaluation of regional block success

PI was originally employed as a predictor of the effectiveness of regional anaesthesia, with a rise in PI being used to identify vasodilation brought on by the suppression of sympathetic tone. In contrast to MAP and skin temperature, PI measured at the toe has been reported as the most sensitive and early predictor of successful sympathectomy and epidural anaesthesia [21, 40]. It has also been shown that PI modification is useful in paediatric patients undergoing general anaesthesia following neuraxial anaesthesia [23, 41, 42, 43].

• PI in evaluation of neuraxial anaesthesiainduced haemodynamic variations

A correlation was found (r = 0.66)between the fall in systolic arterial pressure and basal PI measured at the finger site in parturients undergoing caesarean birth following spinalepidural anaesthesia [44]. In addition, baseline PI had a stronger relationship with a drop in MAP or systolic arterial pressure than baseline heart rate, MAP, or systolic arterial pressure. The optimum threshold value for baseline PI to predict arterial hypotension during spinal-epidural anaesthesia (defined as fall in systolic arterial pressure 25%) was 3.5%, and the area under the receiver operating characteristics curve for this prediction was 0.87 (95% CI 0.74-0.99, p 0.001). Subsequent research vielded similar findings using the same cut-off value [45]. Therefore, a pre-spinal anaesthesia PI value of more than 3.5% indicates a higher risk of anesthesia-induced hypotension. Given that vascular tone is one of the primary drivers of diastolic arterial pressure, one should anticipate that the baseline PI value would likewise precisely predict the drop in diastolic arterial pressure. None of these investigations, however, examined the relationship between baseline PI concentrations and the drop in diastolic arterial pressure. Low basal vascular tone is indicated by a high PI value at baseline. Consequently, in patients with low basal



sympathetic tone, the drop in sympathetic tone brought on by spinal epidural is more likely to cause a decrease in the stressed volume, which in turn causes a decrease in SV and venous return. Therefore, PI is an easy-to-use measure for identifying parturient individuals who are at a high risk of arterial hypotension following spinal anaesthesia and have low sympathetic tone [46].

• Prognosis and PI in anaesthesia

Even after controlling for confounding factors, a sizable, recent, retrospective investigation demonstrated that intraoperative PI was timedependently related to serious postoperative complications or mortality (lower levels being linked with poorer outcomes) [47]. It is yet to be determined if PI targeting during anaesthesia could enhance patient outcomes in randomised controlled studies.

- Clinical uses in Critical Care (Emergency department and ICU)
- PI's Static and dynamic values in ICU patients

More than 15 years ago, Lima et al. published the first research assessing PI in ICU [15]. It assessed how PI changed in critically sick patients with poor peripheral perfusion (i.e., capillary refill time > 2 sec or central-to-toe temperature differential 7 °C) as well as healthy volunteers. The authors of this study found a substantial linear link between changes in PI and the core-to-toe temperature differential as well as a significant exponential relationship between PI and the temperature difference.

• PI and prognosis in Critical Care (Emergency department and ICU)

In patients experiencing acute circulatory a number of investigations have failure. demonstrated the detrimental effects of persistent macrohaemodynamic and/or microcirculatory changes [48-50]. Therefore, it is highly predicted that PI readings or fluctuations would suggest significant and/or chronic circulatory disturbances in these individuals, with greater levels of sympathetic activation. Consequently, this concept has been validated by several studies, and the prognostic significance of PI has been assessed in critically sick patients across various clinical contexts (septic patients, post-cardiac arrest, hypoperfusion patients, emergency department patients, and newborns). PI values in the ICU enable differentiation between septic and nonseptic patients as well as between survivors and non-survivors in various groups (e.g., septic patients, mechanically ventilated patients, etc.) [51]. Additionally, ICU mortality was substantially correlated with PI [51, 52]. After eight hours of resuscitation, PI was able to predict 30-day mortality in hypoperfusion patients more accurately than central venous oxygen saturation (ScvO2), lactate, and arteriovenous carbon dioxide gradient (P(v-a) CO2) [53]. Subgroup analysis revealed that, even after ScvO2 normalisation, PI (with a 0.6% cut-off) could be able to identify patients with the poorest prognosis and identify them for supplementary therapy, particularly those that target the microcirculation. This was supported by a recent study that found that after six hours after resuscitation. survivors' ΡI values were considerably greater than those of non-survivors', indicating that a rise in PI value during the first few hours of resuscitation is linked to a better prognosis [54]. It is hard to determine, nevertheless, if the microcirculation improvement in or macrohaemodynamics-that is, the cardiac indexis the primary cause of the observed difference in PI between survivors and non-survivors following first resuscitation. A prospective investigation has established the possible predictive significance of peripheral PI following cardiac arrest [55]. In this investigation, at day 30, within the first half-hour following the restoration to spontaneous circulation, PI was likewise considerably greater in survivors than in nonsurvivors. The same authors reported similar outcomes once again [56], with patients with greater PI showing longer survival and satisfactory neurologic function (cerebral performance categories \leq 2). However, it is challenging to interpret the PI differences between survivors and non-survivors since the authors did disclose the cardiac index or other not characteristics, such as microcirculation variables. Performances of PI were assessed in a prospective trial for the purpose of triaging patients brought to the emergency room in order to estimate their mortality at 15 and 30 days [57]. In this investigation, PI had no bearing on mortality or hospital admission prediction.

In contrast to ICU patients, this population's low severity rate and poor PI power may account for this.

For the 24 hours following admission, a low PI (\leq 1.4%), as reported in newborns, was proven to be accurate in determining the severity of the disease [58,59]. More information on PI levels in pre-term babies was recently provided by a prospective



research [60]. Therefore, PI appears promising in newborns and babies to quickly assess the severity of disease, and has already become the subject of a review [61].

The majority of studies are retrospective, with PI measurement at various time points and different cut-off values; as a result, the clinical use of PI as a prognostic tool needs more research, even though PI appears effective in differentiating septic from non-septic patients and survivors from non-survivors in the intensive care unit.

• Dynamic changes of PI induced by heat

In a more recent study, individuals arriving with a shock were monitored for microvascular responsiveness using PI and a heating challenge [62]. In comparison to shocked patients, healthy volunteers' PI at the earlobe was substantially greater. All non-septic patients (healthy volunteers, ICU-control patients, and nonseptic shocked patients, i.e., cardiogenic and hemorrhagic) showed a comparable rise in PI value following the heating challenge. After the heating challenge, PI increased less in individuals experiencing septic shock than in non-septic patients. A non-significant trend was seen in the development of PI and PImax/min following the heating challenge in survivors as opposed to nonsurvivors in a small population. Physicians may be able to distinguish between septic and non-septic patients using PI changes and recognise individuals who have a bad prognosis.

Van Genderen et al. examined peripheral tissue perfusion, particularly utilising PI before and after rewarming, in a prospective observational research including patients undergoing therapeutic hypothermia following cardiac arrest [63].

- Fluid Responsiveness
- PI and prediction of fluid responsiveness or fluid removal in ICU

Using a passive leg-raising (PLR) test, Beurton et al. evaluated whether PI fluctuation could reliably predict fluid responsiveness in intensive care unit (ICU) patients, the majority of whom were on mechanical ventilation [32]. With an area under the receiver operating characteristics curve of 0.89 (95% CI 0.8–0.95), a sensitivity of 91% (95% CI 76–98%), a specificity of 79% (95% CI 63–90%), and an increase of PI > 9% generated by PLR predicted an increase in cardiac index > 10% induced by PLR. A further research that also shown that PI fluctuations during an end-expiratory occlusion test might aid in the prediction of positive PLR supported these findings [33]. Regarding spontaneous fluctuations in PI, the cutoff value of the relative PI rise during the endexpiratory occlusion test was; however, much lower (2.5%) than the PI values that are often shown on monitors today, which typically have just one decimal place. In order to predict weaning failure, other scientists used the similar association between PI and SV to study mechanically ventilated patients during a trial of spontaneous breathing (using the ratio of PI before weaning trial/PI during weaning trial) [64]. They noticed that trial failure was linked to a lack of rise in PI during the spontaneous breathing experiment. This shows that patients may be on the early vertical section of the Franck-Starling curve, i.e., fluid responders, when PI increases during the spontaneous breathing trial, and are hence at a decreased risk of weaning-induced pulmonary oedema. Additionally, during renal replacement treatment, PI and PI fluctuations have been utilised to predict hypotension during fluid withdrawal [65].

• PI respiratory variations and prediction of fluid responsiveness

Because deep general anaesthesia lowers the oscillatory components of the perfusion signal linked to sympathetic, myogenic, and endotheliummodulated activity, the variability of PI is modest under steady-state circumstances [66]. Thus, in this case, stroke volume fluctuations are mostly responsible for PI variations. PVI (Pleth Variability Index), also known as PI respiratory variations, has been extensively researched for its capacity to predict fluid responsiveness in patients on mechanical ventilation, particularly in the operating room. The tracking of PI changes as a stand-in for SV variations (or pulse pressure) brought on by positive pressure breathing forms the basis of the physiological concept.

Then, PI respiratory changes may be almost as accurate as pulse pressure variation in predicting fluid responsiveness [67, 68].

In order to estimate fluid responsiveness, a recent meta-analysis by Liu et al. showed that the PVI cut-off value, which ranges from 7% to 20%, depends on the population under study and the ventilation settings (such as an ICU, tidal volume, or positive end expiratory pressure) [69].

Additionally, PVI is significantly impacted by the measurement location (because it is derived from PI) and appears to be a more accurate predictor of fluid responsiveness when



measured in the forehead, as opposed to the finger and earlobe, where it is less affected by vasomotor tone [70]. While a prior research demonstrated lower lactate levels and intraoperative fluid volume when employing PVI-guided fluid management, a recent randomised controlled trial that compared conventional management to hemodynamic peroperative management based on PVI value did not result in a shorter recovery period [71,72]. Consequently, more research is required to determine the significance of PVI value in the OT's hemodynamic management.

In the operating room, PVI may also be a reliable indicator of a child's fluid responsiveness when they are on mechanical breathing [73]. However, the outcomes of the studies conducted on children are inconsistent, necessitating more research to validate the precision of PVI in forecasting fluid responsiveness in the paediatric population [73–75].

• Impact of PI use in haemodynamic management during anaesthesia

It is still unclear if using PI for hemodynamic monitoring will enhance the prognosis of patients having surgery, even if evidence indicate that it is beneficial in this regard. There haven't been any well-planned research done up to now. An intriguing study described how an algorithm integrating pulse pressure variation and PI was used to guide the use of vasopressors and fluid administration (that is, in the event of a hypotension episode, fluids should be given if the PI value stayed constant for the fifteen minutes prior to the hypotension, and on the other hand, an increase in PI value should prompt the use of vasopressors). The application of this strategy was intraoperative linked to decreased fluid administration (4.3 \pm 1.3 ml/kg/h vs. 7.2 \pm 3.3 ml/kg/h, p = 0.003) and decreased arterial hypotension duration $(7.7 \pm 5.0 \text{ min vs. } 17.1 \pm 10.6 \text{ min vs. }$ min, p = 0.003) [76]. Nonetheless, there are a number of issues with this study. Among other things, the control group did not have an algorithm, and the algorithm's use could have encouraged the early use of vasopressors rather than fluid challenge. We may presume that the results of another method with other variables and no PI would be comparable.

• Impact of PI use in haemodynamic management in ICU

PI and its early fluctuations are related to prognosis in the ICU. Particularly in septic patients,

hemodynamic circumstances can be complicated, and PI can be challenging to interpret [35]. The reduced rise in PI following the heating challenge in septic patients suggests that PI might possibly represent microcirculation abnormalities [62]. Rapid PI variations studies, however, are still helpful in ICU patients with maintained microcirculation when one PI variable (such as PLR, fluid challenge, etc.) varies more than the Comparing the PI value others. across measurement sites may offer helpful insights about local perfusion; after all, certain regions may continue to have inadequate perfusion even after their macrohaemodynamic state (MAP, cardiac index, and ScvO2) returns to normal. Recently, we reported on the use of a modified urine catheter for urethral PI monitoring [77]. A steady, dependable signal that could gauge the perfusion of urethral tissue was provided via urethral PI monitoring. But in this study, we didn't particularly assess the impact of therapies (such fluid challenge, vasopressors, and blood transfusion) on PI value, nor did we compare urethral PI value with other measurement locations. Van Genderen et al. observed a trend towards less fluid administration and less organ dysfunction at 72 hours compared with a conventional regimen in a proof of concept study comparing an early peripheral perfusionguided fluid therapy vs. standard of care in patients with septic shock (using capillary refill time, PI, skin temperature difference between forearm and fingertip, and tissue oxygen saturation) [78]. Hernandez et al. have confirmed these results through Bayesian reanalysis of а the ANDROMEDA-SHOCK Trial. They concluded that. in comparison to a lactate-targeted resuscitation strategy, peripheral perfusion-targeted resuscitation-that is, resuscitation guided by capillary refill time—may result in a lower 28-day mortality [79]. In the intensive care unit, resuscitation algorithms that use PI for tissue perfusion evaluation have also been presented [80]. Large-scale randomised controlled studies should evaluate the effects of such algorithms, which include PI, on the outcomes of critically sick patients in conjunction with other resuscitation objectives (e.g., cardiac index, mean arterial pressure, ScvO2, capillary refill time). But under these intricate circumstances (septic shock, hemorrhagic shock, etc.), a number of PI determinants (such as an increase in stoke volume brought on by fluid loading, a rise in vascular tone brought on by vasopressors, and/or the administration of inotropic drugs) may change all



at once and suddenly. This might be a factor in PI's sudden and intricate alterations. In these circumstances, it is more likely that PI changes will be interpreted more properly as an early warning that calls for a reevaluation of the patient's hemodynamic condition, including stroke volume.

II. CONCLUSIONS

The majority of devices now provide PI, a PPG-derived variable that measures perfusion at the interface of central and peripheral perfusion. It seems to be a practical, non-invasive supplementary tool for doctors doing hemodynamic monitoring in anaesthesia, perioperative care, and critical care. Understanding its determinants is essential to understanding its variations. It is yet unknown if PI usage in resuscitation algorithms will lead to better patient outcomes.

REFERENCES

- [1]. Aoyagi T. Pulse oximetry: its invention, theory, and future. Journal of Anesthesia 2003;17:259–66. https://doi.org/10.1007/s00540-003-0192-6.
- [2]. Alian AA, Shelley KH. Photoplethysmography. Best Practice & Research Clinical Anaesthesiology 2014;28:395–406. https://doi.org/10.1016/j.bpa.2014.08.006.
- [3]. Reisner A, Shaltis PA, McCombie D, Asada HH. Utility of the photoplethysmogram in circulatory monitoring. Anesthesiology 2008;108:950–8. <u>https://doi.org/10.1097/ALN.0b013e3181</u> <u>6c89e1</u>.
- [4]. Elgendi M. Optimal Signal Quality Index for Photoplethysmogram Signals. Bioengineering 2016;3:21. <u>https://doi.org/10.3390/bioengineering304</u> 0021.
- [5]. Korhonen I, Yli-Hankala A. Photoplethysmography and nociception. Acta Anaesthesiologica Scandinavica 2009;53:975–85. <u>https://doi.org/10.1111/j.1399-6576.2009.02026.x.</u>
- [6]. Allen J. Photoplethysmography and its application in clinical physiological measurement. Physiological Measurement 2007;28:R1–39. <u>https://doi.org/10.1088/0967-3334/28/3/R01</u>.

- [7]. Murray WB, Foster PA. The peripheral pulse wave: information overlooked. J Clin Monit 1996;12:365–77.
- [8]. Plethsmographic waveform shapes displayed by oximeters-Technical note 2008.
- [9]. PHILIPS. IntelliVue Patient Monitor Philips FAST-SpO2: Application Note n.d.
- [10]. Nijboer JA, Dorlas JC, Mahieu HF. Photoelectric plethysmography--some fundamental aspects of the reflection and transmission method. Clin Phys Physiol Meas 1981;2:205–15.
- [11]. Fine J, Branan KL, Rodriguez AJ, Boonya-ananta T, Ajmal, Ramella-Roman JC, et al. Sources of Inaccuracy in Photoplethysmography for Continuous Cardiovascular Monitoring. Biosensors 2021;11:126. https://doi.org/10.3390/bios11040126.

[12]. Goldman JM, Petterson MT, Kopotic RJ, Barker SJ. Masimo signal extraction pulse oximetry. Journal of Clinical Monitoring and Computing 2000;16:475–483.

[13]. Sang-Soo Oak, Praveen Aroul. How to Design Peripheral Oxygen Saturation (SpO2) and Optical Heart Rate Monitoring (OHRM) Systems Using the AFE4403. 2015.

- [14]. Colquhoun DA, Forkin KT, Durieux ME, Thiele RH. Ability of the Masimo pulse CO-Oximeter to detect changes in hemoglobin. J Clin Monit Comput 2012;26:69–73. <u>https://doi.org/10.1007/s10877-012-9335-3</u>.
- [15]. Lima AP, Beelen P, Bakker J. Use of a peripheral perfusion index derived from the pulse oximetry signal as a noninvasive indicator of perfusion. Critical Care Medicine 2002;30:1210–1213.
- [16]. Keller G, Cassar E, Desebbe O, Lehot J-J, Cannesson M. Ability of pleth variability index to detect hemodynamic changes induced by passive leg raising in spontaneously breathing volunteers. Crit Care 2008;12:R37. <u>https://doi.org/10.1186/cc6822.</u>
- [17]. Nitzan M, Faib I, Friedman H. Respiration-induced changes in tissue blood volume distal to occluded artery, measured by photoplethysmography. J



Biomed Opt 2006;11:040506. https://doi.org/10.1117/1.2236285.

- [18]. Shelley KH. Photoplethysmography: beyond the calculation of arterial oxygen saturation and heart rate. Anesth Analg 2007;105:S31-36, tables of contents. <u>https://doi.org/10.1213/01.ane.000026951</u> 2.82836.c9.
- [19]. Jeong I, Jun S, Um D, Oh J, Yoon H. Non-Invasive Estimation of Systolic Blood Pressure and Diastolic Blood Pressure Using Photoplethysmograph Components. Yonsei Med J 2010;51:345. https://doi.org/10.3349/ymj.2010.51.3.345
- [20]. Galvin EM, Niehof S, Verbrugge SJ, Maissan I, Jahn A, Klein J, et al. Peripheral Flow Index Is a Reliable and Early Indicator of Regional Block Success: Anesthesia & Analgesia 2006;103:239–43. <u>https://doi.org/10.1213/01.ane.000022094</u> 7.02689.9f.
- [21]. Ginosar Y, Weiniger CF, Meroz Y, Kurz V, Bdolah-Abram T, Babchenko A, et al. Pulse oximeter perfusion index as an early indicator of sympathectomy after epidural anesthesia. Acta Anaesthesiologica Scandinavica 2009;53:1018–26. <u>https://doi.org/10.1111/j.1399-6576.2009.01968.x</u>.
- [22]. Kus A, Gurkan Y, Gormus SK, Solak M, Toker K. Usefulness of perfusion index to detect the effect of brachial plexus block. Journal of Clinical Monitoring and Computing 2013;27:325–8. <u>https://doi.org/10.1007/s10877-013-9439-</u> <u>4</u>.
- [23]. Uemura A, Yagihara M, Miyabe M. Pulse oxymeter perfusion index as a predictor for the effect of pediatric epidural block. Anesthesiology 2006;105:A1354.
- [24]. Sebastiani A, Philippi L, Boehme S, Closhen D, Schmidtmann I, Scherhag A, et al. Perfusion index and plethysmographic variability index in patients with interscalene nerve catheters. Canadian Journal of Anesthesia/Journal Canadien d'anesthésie 2012;59:1095–101. <u>https://doi.org/10.1007/s12630-012-9796-3</u>.
- [25]. Coutrot M, Joachim J, Dépret F, Millasseau S, Nougué H, Matéo J, et al. Noninvasive continuous detection of

arterial hypotension during induction of anaesthesia using a photoplethysmographic signal: proof of concept. British Journal of Anaesthesia 2019;122:605– 12. https://doi.org/10.1016/j.bja.2019.01.037.

- [26]. Corsini I, Cecchi A, Coviello C, Dani C. Perfusion index and left ventricular output correlation in healthy term infants. Eur J Pediatr 2017;176:1013–8. <u>https://doi.org/10.1007/s00431-017- 2920-</u> <u>1</u>.
- [27]. Janaillac M, Beausoleil TP, Barrington KJ, Raboisson M-J, Karam O, Dehaes M, et al. Correlations between near-infrared spectroscopy, perfusion index, and cardiac outputs in extremely preterm infants in the first 72 h of life. Eur J Pediatr 2018;177:541–50. https://doi.org/10.1007/s00431-018-3096z.
- [28]. Takahashi S, Kakiuchi S, Nanba Y, Tsukamoto K, Nakamura T, Ito Y. The perfusion index derived from a pulse oximeter for predicting low superior vena cava flow in very low birth weight infants. Journal of Perinatology 2010;30:265–269.
- [29]. van Genderen ME, Bartels SA, Lima A, Bezemer R, Ince C, Bakker J, et al. Peripheral Perfusion Index as an Early Predictor for Central Hypovolaemia in Awake Healthy Volunteers: Anesthesia & Analgesia 2013;116:351–6. <u>https://doi.org/10.1213/ANE.0b013e3182</u> 74e151.
- [30]. Tapar H, Karaman S, Dogru S, Karaman T, Sahin A, Tapar GG, et al. The effect of patient positions on perfusion index. BMC Anesthesiol 2018;18:111. https://doi.org/10.1186/s12871- 018-0571z.
- [31]. Højlund J, Agerskov M, Clemmesen CG, Hvolris LE, Foss NB. The Peripheral Perfusion Index tracks systemic haemodynamics during general anaesthesia. J Clin Monit Comput 2019. <u>https://doi.org/10.1007/s10877-019-</u>00420-x.
- [32]. Beurton A, Teboul J-L, Gavelli F, Gonzalez FA, Girotto V, Galarza L, et al. The effects of passive leg raising may be detected by the plethysmographic oxygen saturation signal in critically ill patients. Crit Care 2019;23:19.



https://doi.org/10.1186/s13054-019-2306-

- Z. [33]. Beurton A, Gavelli F, Teboul J-L, De Vita N, Monnet X. Changes in the Plethysmographic Perfusion Index During an End-Expiratory Occlusion Detect a Positive Passive Leg Raising Test*. Critical Care Medicine 2021;49:e151–60. <u>https://doi.org/10.1097/CCM.0000000000</u> <u>004768</u>.
- [34]. Lian H, Wang X, Zhang Q, Zhang H, Liu D. Changes in perfusion can detect changes in the cardiac index in patients with septic shock. J Int Med Res 2020;48:030006052093167. https://doi.org/10.1177/030006052093167 <u>5</u>.
- [35]. He H-W, Liu W-L, Zhou X, Long Y, Liu D-W. Effect of mean arterial pressure change by norepinephrine on peripheral perfusion index in septic shock patients after early resuscitation. Chin Med J (Engl) 2020;133:2146–52. https://doi.org/10.1097/CM9.0000000000 001017.
- [36]. Charkoudian N. Mechanisms and modifiers of reflex induced cutaneous vasodilation and vasoconstriction in humans. Journal of Applied Physiology 2010;109:1221–8. https://doi.org/10.1152/japplphysiol.00298 .2010.
- [37]. Hodges GJ, Johnson JM. Adrenergic control of the human cutaneous circulation. Appl Physiol Nutr Metab 2009;34:829–39.
 - https://doi.org/10.1139/H09-076.
- [38]. Awad AA, Ghobashy MA, Ouda W, Stout RG, Silverman DG, Shelley KH. Different responses of ear and finger pulse oximeter wave form to cold pressor test. Anesth Analg 2001;92:1483–6. <u>https://doi.org/10.1097/00000539-</u> 200106000-00026.
- [39]. Shelley KH, Tamai D, Jablonka D, Gesquiere M, Stout RG, Silverman DG. The Effect of Venous Pulsation on the Forehead Pulse Oximeter Wave Form as a Possible Source of Error in Spo2 Calculation: Anesthesia & Analgesia 2005;100:743–7. https://doi.org/10.1213/01.ANE.00001450 <u>63.01043.4B</u>.

- [40]. Kakazu CZ, Chen B-J, Kwan W-F. Masimo set technology using perfusion index is a sensitive indicator for epidural onset. Anesthesiology 2005;103:A576.
- [41]. Xu Z, Zhang J, Xia Y, Deng X. Accuracy of pulse oximeter perfusion index in thoracic epidural anesthesia under basal general anesthesia. International Journal of Clinical and Experimental Medicine 2014;7:1728.
- [42]. Abdelhamid B, Emam M, Mostafa M, Hasanin A, Awada W, Rady A, et al. The ability of perfusion index to detect segmental ulnar nerve sparing after supraclavicular nerve block. J Clin Monit Comput 2019. <u>https://doi.org/10.1007/s10877-019-00443-4</u>.
- [43]. Kim D, Jeong JS, Park MJ, Ko JS. The effect of epinephrine on the perfusion index during ultrasound-guided supraclavicular brachial plexus block: a randomized controlled trial. Sci Rep 2020;10:11585. https://doi.org/10.1038/s41598-020-68475-4.
- [44]. Toyama S, Kakumoto M, Morioka M, Matsuoka K, Omatsu H, Tagaito Y, et al. Perfusion index derived from a pulse oximeter can predict the incidence of hypotension during spinal anaesthesia for Caesarean delivery. British Journal of Anaesthesia 2013;111:235–41. https://doi.org/10.1093/bja/aet058.
- [45]. Duggappa D, Lokesh M, Dixit A, Paul R, Raghavendra Rao R, Prabha P. Perfusion index as a predictor of hypotension following spinal anaesthesia in lower segment caesarean section. Indian J Anaesth 2017;61:649. https://doi.org/10.4103/ija.IJA_429_16.
- [46]. Hager H., Church S., Mandadi G., Pulley D. The Perfusion Index as Measured by a Pulse Oximeter Indicates Pain Stimuli in Anesthetized Volunteers. Anesthesiology 2004;101:A514.
- [47]. Agerskov M, Thusholdt ANW, Holm-Sørensen H, Wiberg S, Meyhoff CS, Højlund J, et al. Association of the intraoperative peripheral perfusion index with postoperative morbidity and mortality in acute surgical patients: a retrospective observational multicentre cohort study. British Journal of



Anaesthesia 2021:S0007091221003561. https://doi.org/10.1016/j.bja.2021.06.004.

- [48]. Sakr Y, Dubois M-J, De Backer D, Creteur J, Vincent J-L. Persistent microcirculatory alterations are associated with organ failure and death in patients with septic shock. Crit Care Med 2004;32:1825–31.
- [49]. Top APC, Ince C, de Meij N, van Dijk M, Tibboel D. Persistent low microcirculatory vessel density in nonsurvivors of sepsis in pediatric intensive care*: Critical Care Medicine 2011;39:8–13. <u>https://doi.org/10.1097/CCM.0b013e3181</u> <u>fb7994</u>.
- [50]. Ait-Oufella H, Lemoinne S, Boelle PY, Galbois A, Baudel JL, Lemant J, et al. Mottling score predicts survival in septic shock. Intensive Care Medicine 2011;37:801–7. https://doi.org/10.1007/s00134-011-2163-v.
- [51]. He H, Liu D, Long Y, Wang X. The peripheral perfusion index and transcutaneous oxygen challenge test are predictive of mortality in septic patients after resuscitation. Crit Care 2013;17:R116.
- <u>https://doi.org/10.1186/cc12788</u>.
 [52]. Su L, Zhang R, Zhang Q, Xu Q, Zhou X, Cui N, et al. The Effect of Mechanical Ventilation on Peripheral Perfusion Index and Its Association With the Prognosis of
- Critically Ill Patients: Critical Care Medicine 2019;47:685–90. https://doi.org/10.1097/CCM.000000000 003661.
- [53]. He H, Long Y, Liu D, Wang X, Zhou X. Clinical classification of tissue perfusion based on the central venous oxygen saturation and the peripheral perfusion index. Crit Care 2015;19:330. <u>https://doi.org/10.1186/s13054-015-1057-8</u>.
- [55]. Savastano S, Baldi E, Molinari S, Canevari F, Corazza V, Cacciatore E, et

al. Post ROSC pulseoximetry derived perfusion index and thirty days survival after out-of-hospital cardiac arrest. New insights from the Pavia CARe (Pavia Cardiac Arrest Registry). Resuscitation 2017;117:e19– 20. <u>https://doi.org/10.1016/j.resuscitation.201</u> 7.05.027.

- [56]. Savastano S, Baldi E, Contri E, De Pirro A, Sciutti F, Compagnoni S, et al. Post-ROSC peripheral perfusion index discriminates 30-day survival after out-ofhospital cardiac arrest. Intern Emerg Med 2020. <u>https://doi.org/10.1007/s11739-020-02430-z</u>.
- [57]. Oskay A, Eray O, Dinç SE, Aydın AG, Eken C. Prognosis of Critically Ill Patients in the ED and Value of Perfusion Index Measurement: A Cross-Sectional Study. The American Journal of Emergency Medicine 2015;33:1042–4. https://doi.org/10.1016/j.ajem.2015.04.033
- [58]. De Felice C, Latini G, Vacca P, Kopotic RJ. The pulse oximeter perfusion index as a predictor for high illness severity in neonates. European Journal of Pediatrics 2002;161:561–2. <u>https://doi.org/10.1007/s00431-002-1042-5</u>.
- [59]. Richardson DK, Gray JE, McCormick MC, Workman K, Goldmann DA. Score for Neonatal Acute Physiology: a physiologic severity index for neonatal intensive care. Pediatrics 1993;91:617–23.
- [60]. Alderliesten T, Lemmers PMA, Baerts W, Groenendaal F, van Bel F. Perfusion Index in Preterm Infants during the First 3 Days of Life: Reference Values and Relation with Clinical Variables. Neonatology 2015;107:258–65. <u>https://doi.org/10.1159/000370192</u>.
- [61]. Piasek CZ, Van Bel F, Sola A. Perfusion index in newborn infants: a noninvasive tool for neonatal monitoring. Acta Paediatr 2014;103:468–73. https://doi.org/10.1111/apa.12574.
- [62]. Vallée F, Nougué H, Mari A, Vodovar N, Dubreuil G, Damoisel C, et al. Variations of Cutaneous Capnometry and Perfusion Index During a Heating Challenge is Early Impaired in Septic Shock and Related to Prognostic in Non-Septic Shock: SHOCK 2019;51:585–92.



4.

https://doi.org/10.1097/SHK.000000000 001216.

- [63]. van Genderen ME, Lima A, Akkerhuis M, Bakker J, van Bommel J. Persistent peripheral and microcirculatory perfusion alterations after out-of-hospital cardiac arrest are associated with poor survival*: Critical Care Medicine 2012;40:2287–94. <u>https://doi.org/10.1097/CCM.0b013e3182</u> 5333b2.
- [64]. Lotfy A, Hasanin A, Rashad M, Mostafa M, Saad D, Mahmoud M, et al. Peripheral perfusion index as a predictor of failed weaning from mechanical ventilation. J Clin Monit Comput 2020. https://doi.org/10.1007/s10877-020-00483-1.
- [65]. Klijn E, Groeneveld ABJ, van Genderen ME, Betjes M, Bakker J, van Bommel J. Peripheral Perfusion Index Predicts Hypotension during Fluid Withdrawal by Continuous Veno-Venous Hemofiltration in Critically Ill Patients. Blood Purif 2015;40:92–8.

https://doi.org/10.1159/000381939.

- [66]. Landsverk SA, Kvandal P, Bernjak A, Stefanovska A, Kirkeboen KA. The Effects of General Anesthesia on Human Skin Microcirculation Evaluated by Wavelet Transform: Anesthesia & Analgesia 2007;105:1012–9. <u>https://doi.org/10.1213/01.ane.000028193</u> 2.09660.96.
- [67]. Chu H, Wang Y, Sun Y, Wang G. Accuracy of pleth variability index to predict fluid responsiveness in mechanically ventilated patients: a systematic review and meta-analysis. J Clin Monit Comput 2016;30:265–74. https://doi.org/10.1007/s10877-015-9742-<u>3</u>.
- [68]. Yang X, Du B. Does pulse pressure variation predict fluid responsiveness in critically ill patients? A systematic review and meta-analysis. Crit Care 2014;18:650. <u>https://doi.org/10.1186/s13054-014-0650-6</u>.
- [69]. Liu T, Xu C, Wang M, Niu Z, Qi D. Reliability of pleth variability index in predicting preload responsiveness of mechanically ventilated patients under various conditions: a systematic review and meta-analysis. BMC Anesthesiol 2019;19:67.

https://doi.org/10.1186/s12871-019-0744-

[70]. Desgranges F-P, Desebbe O, Ghazouani A, Gilbert K, Keller G, Chiari P, et al. Influence of the site of measurement on the ability of plethysmographic variability index to predict fluid responsiveness. British Journal of Anaesthesia 2011;107:329–35.

https://doi.org/10.1093/bja/aer165.

- [72]. Forget P, Lois F, de Kock M. Goal-Directed Fluid Management Based on the Pulse Oximeter– Derived Pleth Variability Index Reduces Lactate Levels and Improves Fluid Management: Anesthesia & Analgesia 2010:1. <u>https://doi.org/10.1213/ANE.0b013e3181e</u> <u>b624f</u>.
- [73]. Desgranges F-P, Evain J-N, Pereira de Souza Neto E, Raphael D, Desebbe O, Chassard D. Does the plethysmographic variability index predict fluid responsiveness in mechanically ventilated children? A meta-analysis. British Journal of Anaesthesia 2016;117:409–10. https://doi.org/10.1093/bja/aew245.
- [74]. Pereira de Souza Neto E. Grousson S. Duflo F, Ducreux C, Joly H, Convert J, et al. Predicting fluid responsiveness in mechanically ventilated children under general anaesthesia using dynamic transthoracic parameters and echocardiography. British Journal of Anaesthesia 2011;106:856-64. https://doi.org/10.1093/bja/aer090.
- [75]. Chen P, Chan K, Liao M, Wu C. Accuracy of dynamic preload variables for predicting fluid responsiveness in patients with pediatric liver cirrhosis: A prospective study. Pediatr Anaesth 2020;30:455–61. https://doi.org/10.1111/pan.13819.

[76]. Godai K, Matsunaga A, Kanmura Y. The effects of hemodynamic management using the trend of the perfusion index and

pulse

pressure variation on

tissue



perfusion: a randomized pilot study. JA Clin Rep 2019;5:72. https://doi.org/10.1186/s40981-019-0291-5.

- [77]. Dépret F, Leone M, Duclos G, Futier E, Montagne M, Legrand M, et al. Monitoring tissue perfusion: a pilot clinical feasibility and safety study of a urethral photoplethysmographyderived perfusion device in high-risk patients. J Clin Monit Comput 2019. <u>https://doi.org/10.1007/s10877-019-</u> 00414-9.
- [78]. van Genderen ME, Engels N, van der Valk RJP, Lima A, Klijn E, Bakker J, et al. Early Peripheral Perfusion-guided Fluid Therapy in Patients with Septic Shock. Am J Respir Crit Care Med 2015;191:477-80. <u>https://doi.org/10.1164/rccm.201408-</u> 1575LE.
- [79]. Zampieri FG, Damiani LP, Bakker J, Ospina-Tascón GA, Castro R, Cavalcanti AB, et al. Effects of a Resuscitation Strategy Targeting Peripheral Perfusion Status versus Serum Lactate Levels among Patients with Septic Shock. A Bayesian Reanalysis of the ANDROMEDA-SHOCK Trial. Am J Respir Crit Care Med 2020;201:423–9. https://doi.org/10.1164/rccm.201905-0968OC.
- [80]. Hariri G, Joffre J, Leblanc G, Bonsey M, Lavillegrand J-R, Urbina T, et al. Narrative review: clinical assessment of peripheral tissue perfusion in septic shock. Ann Intensive Care 2019;9:37. https://doi.org/10.1186/s13613-019-0511-1.